Preparation of advanced bioceramic materials with controlled size using supercritical fluid technology

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EULANetCermat meeting February, 28th 2013

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Ultimate Objective

Preparation of scaffold materials for bone tissue engineering

Development Of TiO₂/Hydroxyapatite Nanoestructured Bioceramics By Using High Pressure Methods.

OUTLINE

Supercritical fluids

Tissue Engineering
Biomaterials
Hydroxyapatite

Methods for the development of porosity

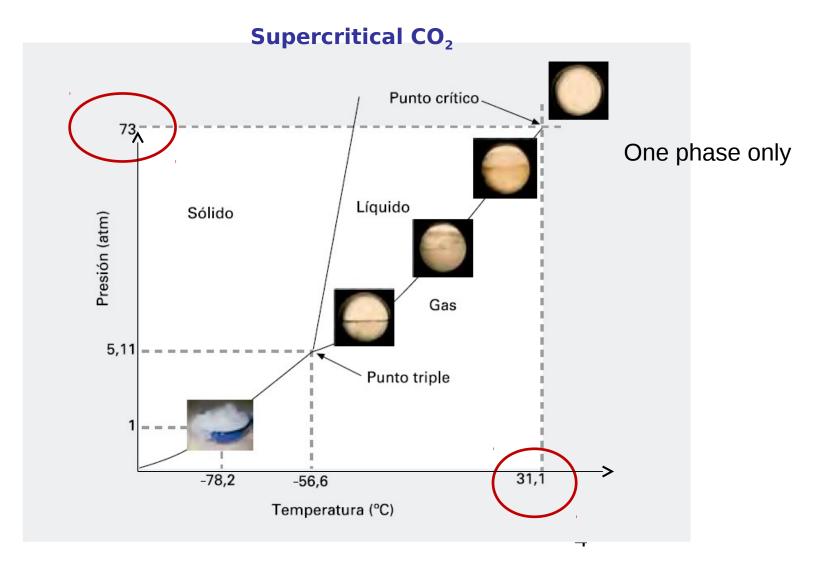
Development Of TiO₂/Hydroxyapatite Nanoestructured Bioceramics

INTEMA-ICMAB approach

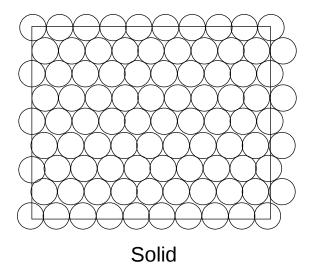


Supercritical Fluid

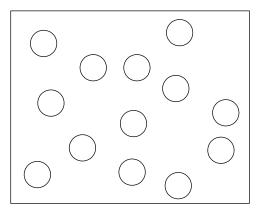
Fluid whose pressure and temperature are above the critical point



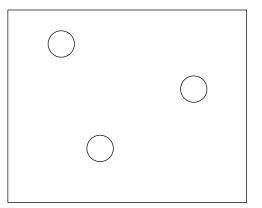
scCO₂ :intermediate between liquids and gases



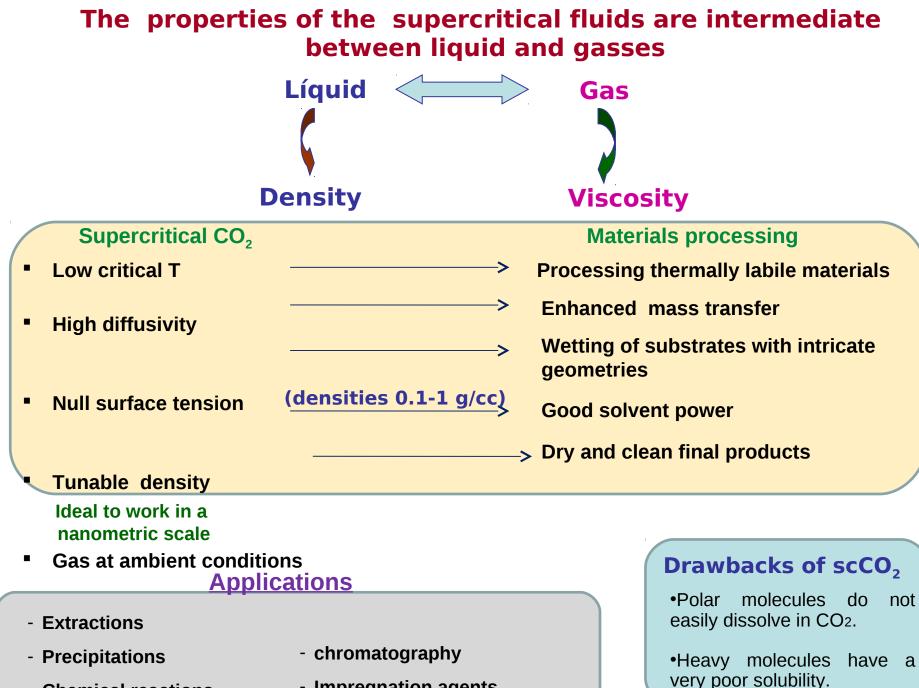
Liquid



Supercritical Fluid



Gas

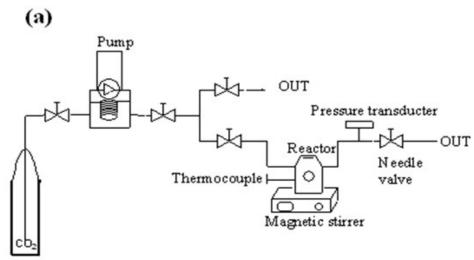


- Chemical reactions

- Impregnation agents....



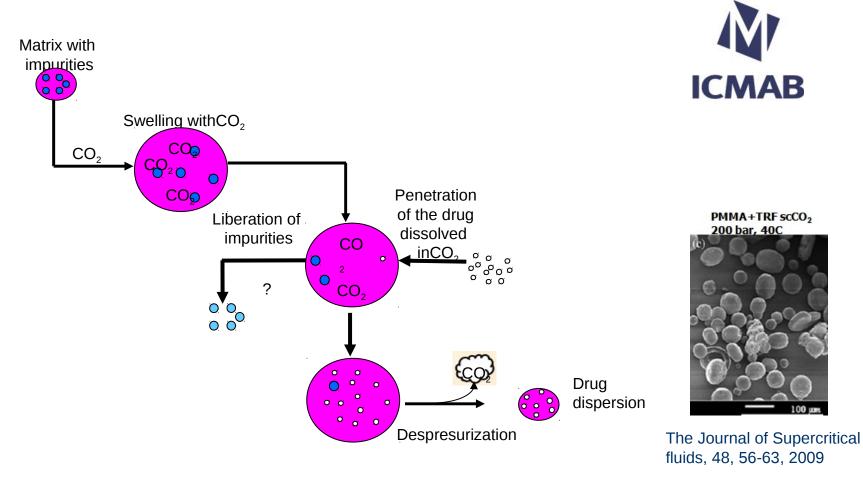




Uses of scCO₂

> Supercritical CO₂ technology has significant potential for solvent replacement

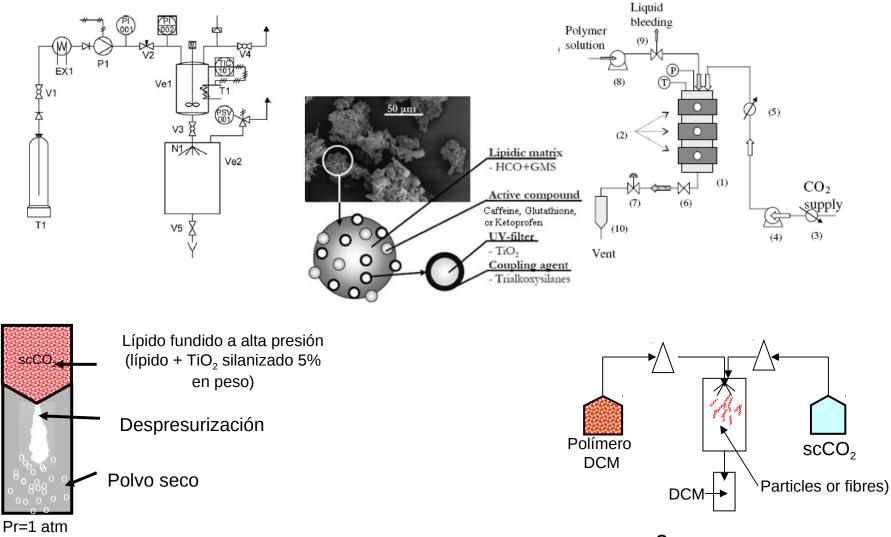
Impregnation of matrices for drug delivery



Nanoparticle and drug carrier preparation

Particles from Gas saturated solutions(PGSS)

Supercritical antisolvent precipitation (SAS)



International Journal of Pharmaceutics 382 (1-2), pp. 296-304

European Por Journal, 44,2008, 081-1094

Industrial applications

Big scale extraction

- \checkmark Decaffeination of Coffee and Tea
- \checkmark Extraction of yeast



Evonik Group: Key figures	Alemania				
in € million	2006	2007	2008	2009	2010
Sales	14,125	14,444	15,873	10,518	13,300



Pittsburgh- EEUU



Holanda











Industria Española









Pharmaceutical and biotechnological Industry

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Development Of TiO₂/Hydroxyapatite Nanoestructured Bioceramics

INTEMA-ICMAB approach

Resources



Properties of Ideal Scaffold- Bone scaffolds

Material Properties

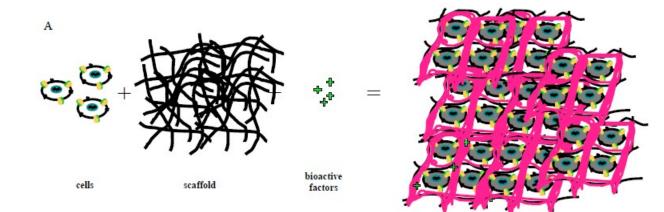
- Structurally strong
- \geq High porosity, high surface area to volume ratio
- Uniformly distributed and interconnected pore structure

-Pore sizes with diameters $150-300\mu$ m are recommended to promote good vascularisation and attachment of bone cells to guide their growth into all three dimensions

Biological Properties

- Biocompatibility
- Promotion of cell adhesion
- Enhancement of cell growth
- **Retention of differentiated cell function**

Preparing a tissue engineered bone



tissue-engineered construct

1. Scaffold

By rapid prot)

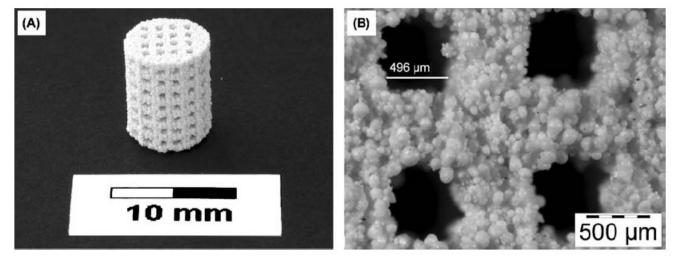
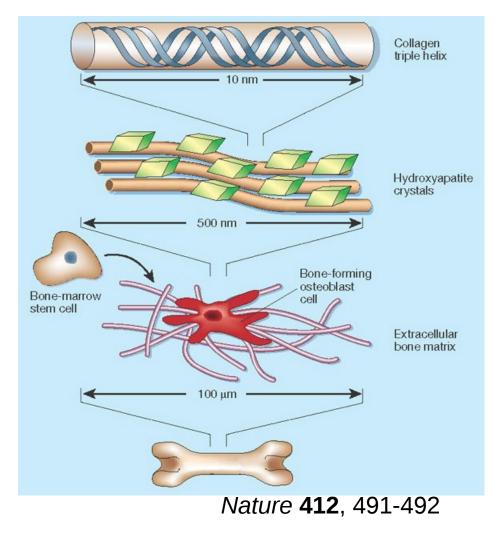


Figure 3 3D printed testpart with interconnecting channels. (a) Whole structure. (b) Detail view of the interconnecting channel structure with diameter of about 500 μ m. The remaining granule structure is visible.

JOURNAL OF MATERIALS SCIENCE: MATERIALS IN MEDICINE 16 (2005) 1121 - 1124

Bone is one example of a natural material whose properties depend intimately on its nanoscale structure



✓ Bone is an inorganic–bioorganic composite material consisting mainly of collagen proteins and hydroxyapatite (a crystalline form of calcium phosphate).

✓ Collagen spontaneously forms fibrils of aligned protein helices, on which tiny hydroxyapatite crystals (10–50 nanometres in length) can grow.

 \checkmark Both the size and the orientation of the crystals are dictated specifically by the collagen template, and the precise structural relationship between the collagen and hydroxyapatite is critical to bone's resilience and strength.

Biomaterials for <u>Tissue Engineering</u>

Scaffolds composition for bone tissue engineered materials are mainly made of bioceramics (Inorganic Ca derivates)

Hydroxyapatite (HAp)

[Ca10(PO4)6(OH)2]

is the natural component of bones

Hydroxyapatite

70% of bone is inorganic mineral hydroxyapatite $[Ca_{10}(PO_4)_6 (OH)_2]$

Predominantly crystalline, though may be present in amorphous forms.

The crystals are platelets or rods, about 8 to 15A thick, 20 to 40A wide and 200 to 400A long.

The substitution mechanisms that occur in the hydroxyapatite of bone include intercrystalline exchange and a recrystallisation due to dissolution and reformation of crystals, with the addition of new ions into the crystal structure replacing Ca2+ or being adsorbed on the crystal surfaces



Hydroxyapatite



Human Bone

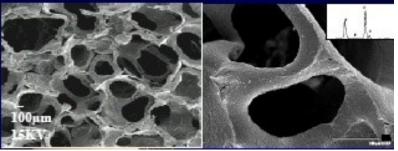
HAp ceramics have some weaknesses such as the poor toughness and low-bending strength.

If density of HAp ceramic mechanical properties bioactivity



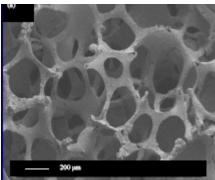


compressive strength of a bone is about 170 MPa



scaffolds are too brittle

Compressive yield stress: 8 MPa



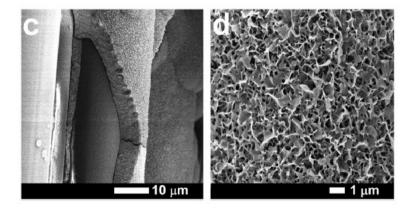
Compressive stress 9.8 MPa

Research current trends

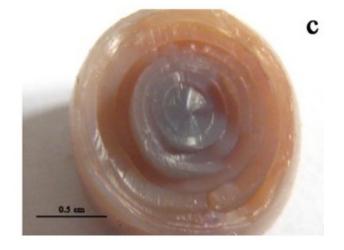
To improve the mechanical properties

Bioabsorbable and bioactive composites have been developed combining resorbable polymers with calcium phosphates, bioactive glasses or glass-ceramics in various scaffold architectures, fibers etc

hydroxyapatite-coated PLLA fibers:



Journal of the Mechanical Behavior of Biomedical Materials, 17, 2013, 269–277 Genipin-crosslinked chitosan/hydroxyapatite composite



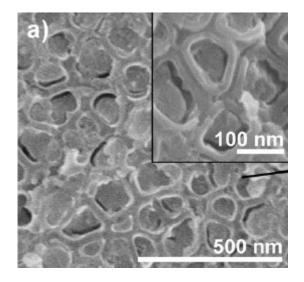
Materials Letters 94 (2013) 169–171 18

Tissue Eng ICMAB Design of scaffolds from HAp/Titanium

 \checkmark Titania composites materials are recognized as one of the best biomaterials for prostheses

 \checkmark The immobilization of a biocompatible metal/metal oxide on the surface of the hydroxyapatite \rightarrow Would improve the cellular responses and biocompatibility of HAp along with high toughness and strength.

TiO₂ nanotube surfaces for site-selective nucleation of hydroxyapatite



Apatite filled tubes at the sample surface

Deposition of HAp in TiO₂. examples

-Design of scaffolds from Titanium intermingled fibres

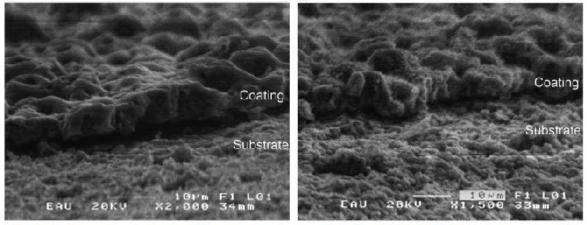
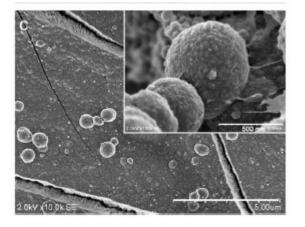


Fig. 2. SEM micrographs showing the thickness and surface morphologies of: (a) ECAE/MAO-treated sample and (b) ECAE/MAO/HT-treated sample.

-Hydroxyapatite production on ultrafine-grained pure titanium. Surf. Coat. Technol. (2011), doi:10.1016/j.surfcoat.2011.03.032.

-Film of TiO₂ nanotubes recovered with calcium phosphates via simply immersion



Characterization of a calcium phosphate-TiO2 nanotube composite layer for biomedical applications. *Mater. Sci. Eng. C* 31 (2011) 906-914.

OUTLINE

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Tissue Engineering
Biomaterials
Hydroxyapatite

Methods for the development of porosity

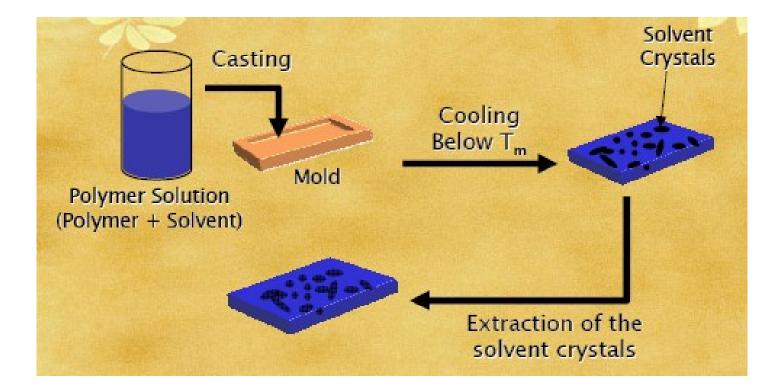
Contract States and S

***** INTEMA-ICMAB approach

Resources

Methods for creating porosity

Thermally Induced Phase Separation

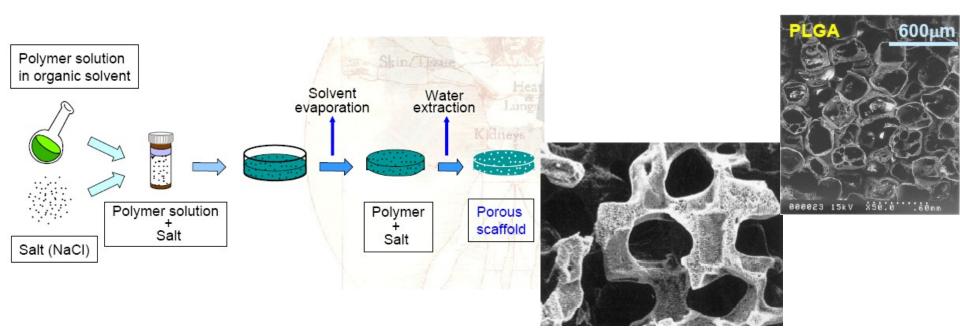


Solvent casting/Particulate leaching

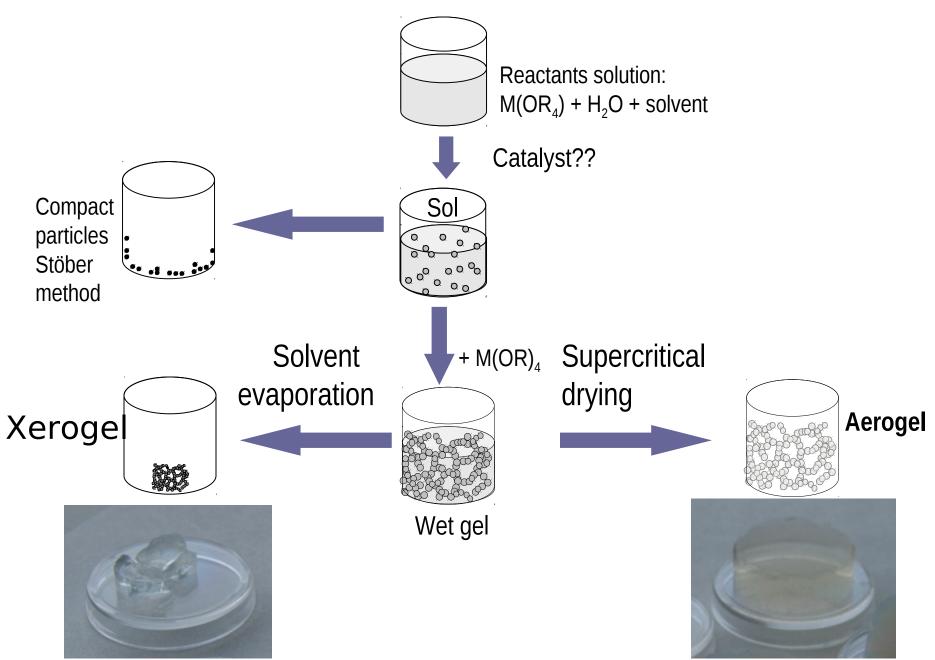
1.- First the material is dissolved into a suitable organic solvent,

- 2.- Then the solution is cast into a mold filled with porogen particles.
- (A salt like sodium chlorid, crystals of saccharose, gelatin or paraffin spheres)
- 4.- After the mixture solution has been cast, the solvent is allowed to fully evaporate

5.- Then the composite structure in the mold is immersed in a bath of a liquid suitable for dissolving the porogen (Water in case of sodium chloride, saccharose and gelatin, or hexane for paraffin)



Supercritical drying with CO₂



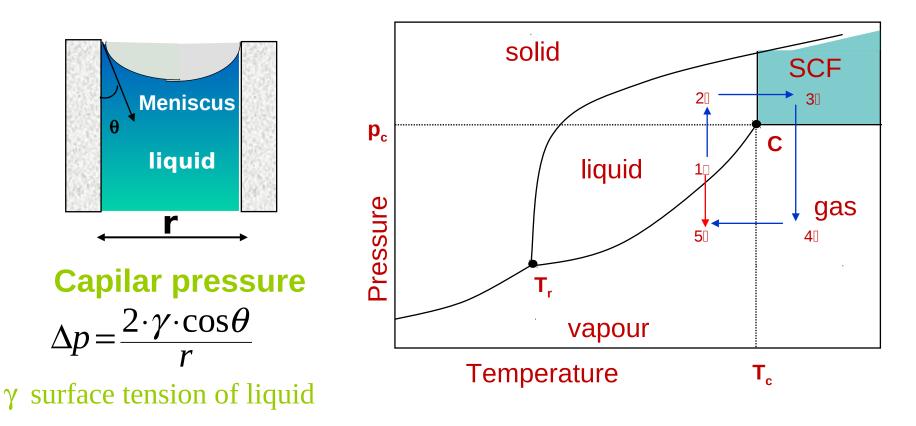


Supercritical Drying

This is where the liquid within the gel is removed, leaving only the linked aerogel network.

vapour-liquid interphase in the pores

supercritical extraction of the solvent



INTEMA-ICMAB approach

Development of porous nanostructured materials of using high pressure technologies

-Hydrothermal synthesis of HAp nanoparticles

-Synthesis of TiO₂ precursor gels

-Synthesis of TiO₂-HAp opened structures through supercritical drying



I-Hydrothermal synthesis of HAp nanoparticles



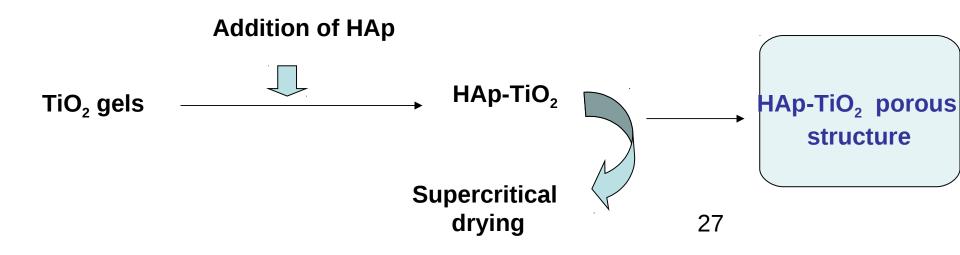
Morphology control of HAp nanoparticles- (nanorods)

II-Synthesis of TiO₂ porous structures



Sol-gel synthesis

III- Synthesis of TiO₂-HAp opened structures



I- Hydrothermal synthesis of HAp nanoparticles

-Hydrothermal synthesis (subcritical conditions in batch reactors) is generally defined as crystal synthesis or crystal growth under high temperature and high pressure water conditions from substances which are insoluble in ordinary temperature and pressure

-Tc(water)=374 °C Pc(Water)= 22.1 MPa

-Hydrothermal synthesis is usually carried out below 300 °C.

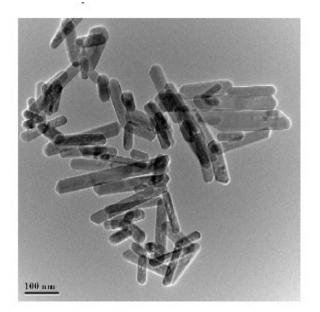


Fig. 2. FETEM image of the HAp nanorods.

K.Ling et al Materials Letters 61 (2007) 1683–1687 28 Hydrothermal microemulsion synthesis of stoichiometric single crystal hydroxyapatite nanorods

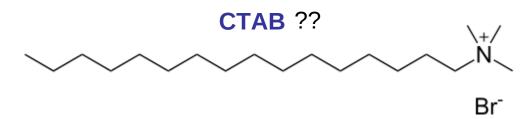
Hydrothermal synthesis of HA nanoparticles

OBTECTIVE: Synthesis of Nanoparticles of (HAp) with particle size control and monodispersity.

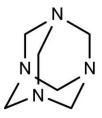
HAp will be prepared from

CaHPO4.2H2O / NaOH / distilled water

Evaluation of the use of different templates:



Hexametilenetetraamine



Evaluation of pH control and Temperature 110-200 C

-Activity under development-



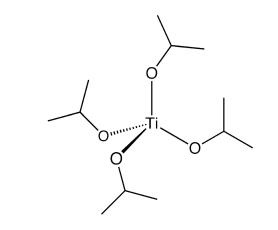
II- Sol-Gel synthesis of TiO₂

Precursors

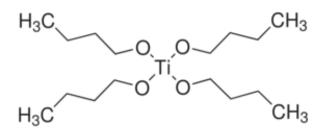
EtOH

Dry box and N2

Titanium isopropoxide



Titanium butoxide



TiOR + $H_2O \rightarrow TiOH + EtOH$ (hydrolysis)

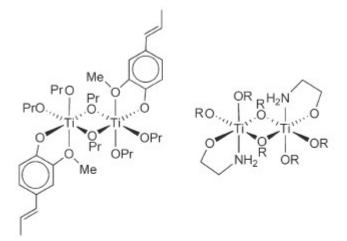
TiOH + HO-Ti -→ Ti-O-Ti + EtOH (condensation) TiOR + TiOH → Ti-O-Ti -Activity under development- Dr. A∓anovich

-Activity under development-

-To delay the polycondensation and prevent the precipitation of titanium Oxi / hydroxydes, The alcoxydes will be modified with chelant ligands or beta-diketones

-Ti(OR)₄ reacts vigorously with water producing titanium-oxo/hydroxy precipitates.

In contrast, when chemical additives are employed, transparent titania-based sols and gels can be obtained.



Addition of water to promote the hydrolysis and condensation to lead to the formation of Ti-O-Ti bonds and the growing of a TiO₂ 3D-network

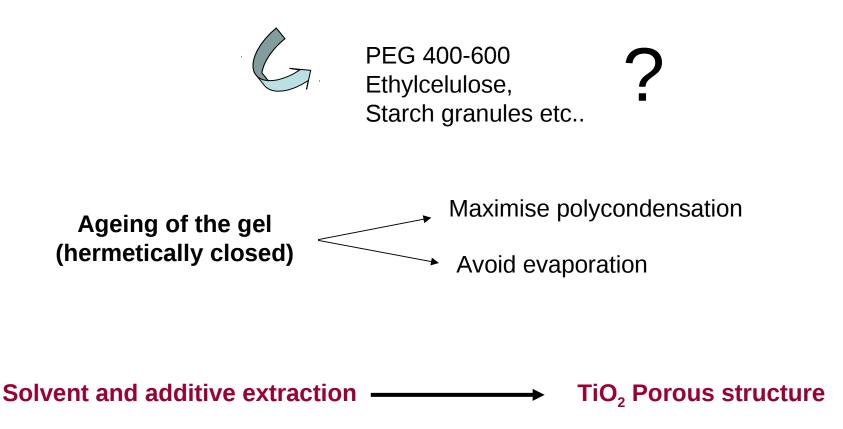
Fig. 4 The structures of $Ti_2(OPr)_6(isoeugenolate)_2$ (left) and $Ti_2(OR)_6(OCH_2CH_2NH_2)_2$ (R = ⁱPr, Et) (right).³⁰

J. Mater. Chem., 2005, 15, 3701–3715 | 3701

Dr. A Fanovich

-Activity under development-

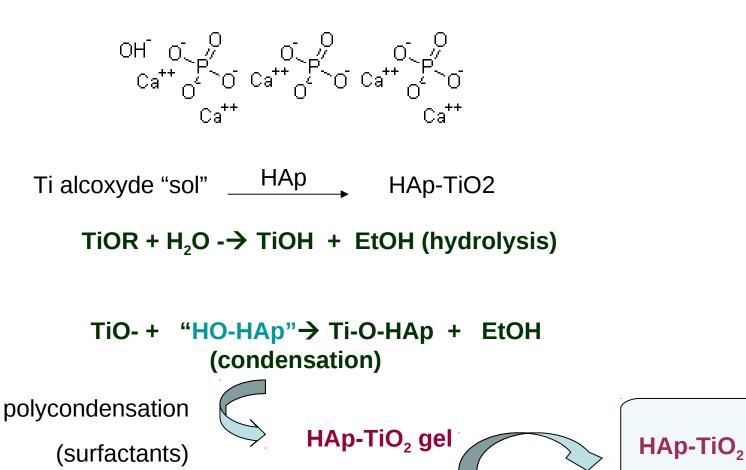
Addition of porous generator agents to the "sol" to allow an open porous micro structure of 150-300 microns



II- Synthesis of HAp-TiO2

Objective: prepara TiO_2/HAp with HAp nanoparticles homogeneously dispersed in a TiO_2

HAp contains –OH groups that can be linked to TiO₂

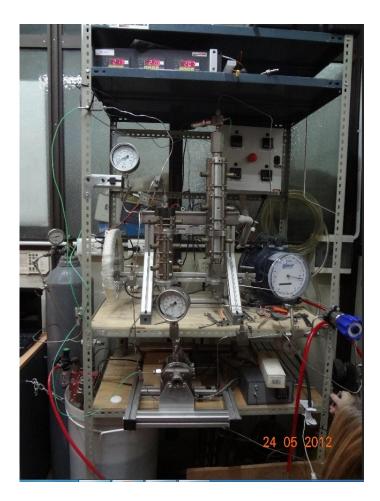


33

Supercritical CO₂









Continuous flow

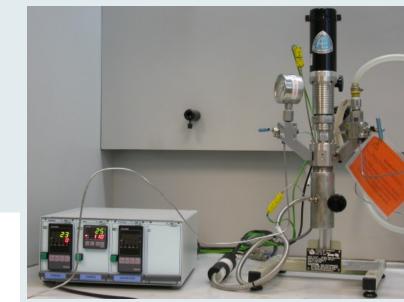


Compresión del gas

Procesamiento de muestras

Expansión del gas

Funcionalization Equipment- Batch







Celda de volumen variable





200 ml





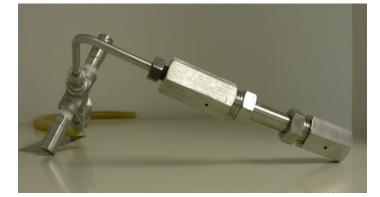
100 ml



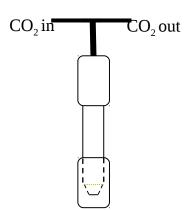


Designed for supercritical-ultrasound research

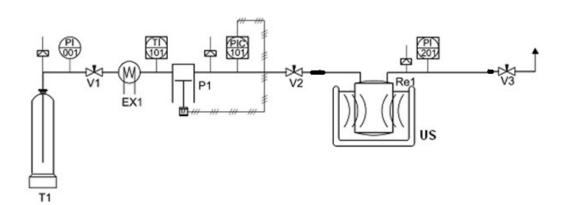
10 ml



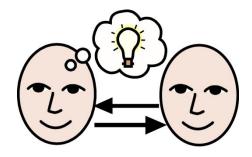
5 ml





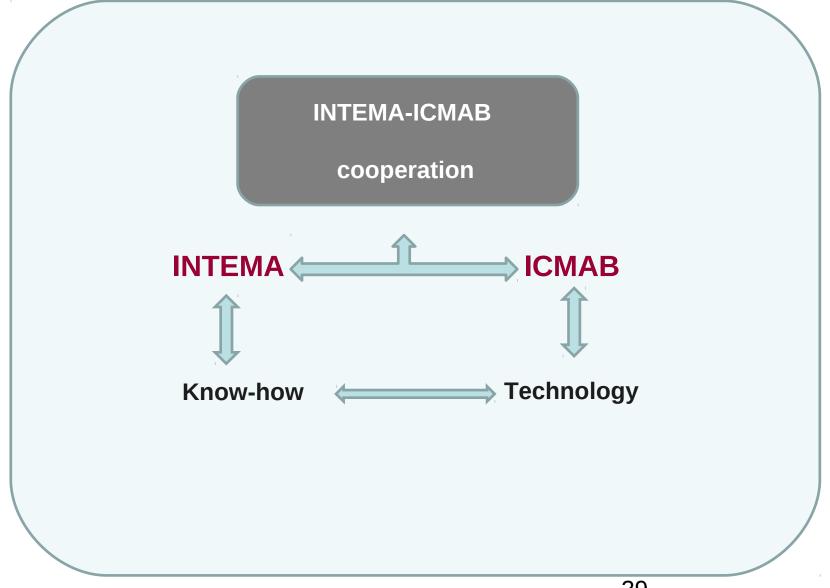


HAp-TiO₂ gels using ultrasonic cavitation??



ICMAB

INTEMA





Characterisation

- -To evaluate homogeneity of aerogels and morphology SEM
- -Raman and DRX to analyse crystallisation and phases
- IR to check purity of the samples
- -BET. Fo size and pore distribution
- -Size distribution- Malvern Nanosizer

Summary

I-Hydrothermal synthesis of HAp nanoparticles

The hydrothermal synthesis allows morphology control of the hydroxyapatite particles.

-Halide precursors and organic templates will be used to promote the growth of HAp nanorods. We will study the effect of the main synthetic parameters on the characteristics of the material obtained.

II-Synthesis of TiO2 gels

Sol-gel synthesis of TiO2 will allow the introduction of porous generator agents.

-The chemicals that will be used are: Ti alcoxydes, EtOH, surfactants, and porous generator agents.

-Precursors condensation will be promoted my the addition of water

- Gels will be aged within their original pot, to avoid evaporation

III- Synthesis of TiO2-HAp opened structures

The HO- groups of the hydroxyapatite particles can condensate with the Titanium alcoxydes to lead to HAp-O-Ti

-polycondensation will result in a aigel composed of HAp nanoparticles anchores in the TiO2 network

Sol-Gel synthesis process

Step 1: Formation of solutionos of alkoxide or solvated metal precursor (the sol).

Step 2: Gelation resulting from the formation of an oxide- or alcohol- bridged network (the gel) by a polycondensation or polyesterification reaction that results in a dramatic increase in the viscocity of the solution.

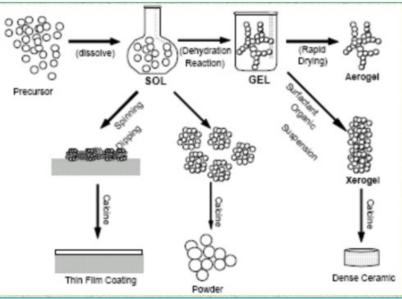
Step 3: Aging of the gel (Syneresis).- polycondensation reactions continue until the gel transforms into a solid mass, -expulsion of solvent from gel pores.

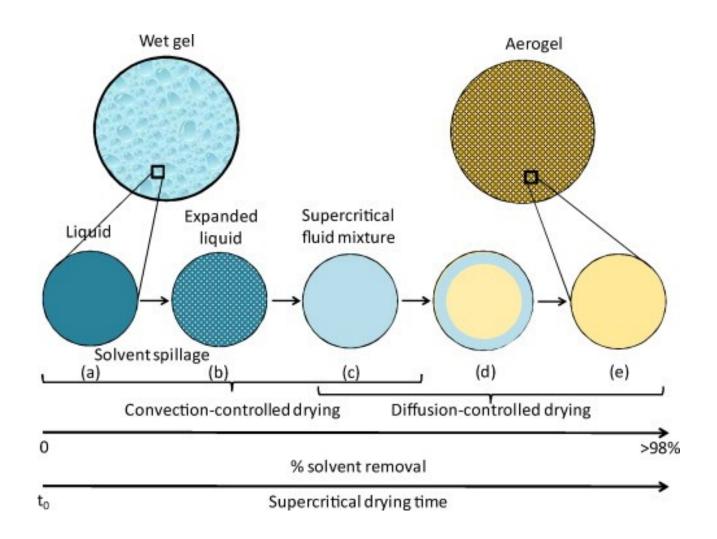
Step 4: Drying of the gel, when water and other volatile liquids are removed from the gel network.

Step 5: Dehydration- Ti-OH groups are removed, there by stabilizing the gel against rehydration. This is normally achieved by calcining the monolith at temperatures up to 8000C.

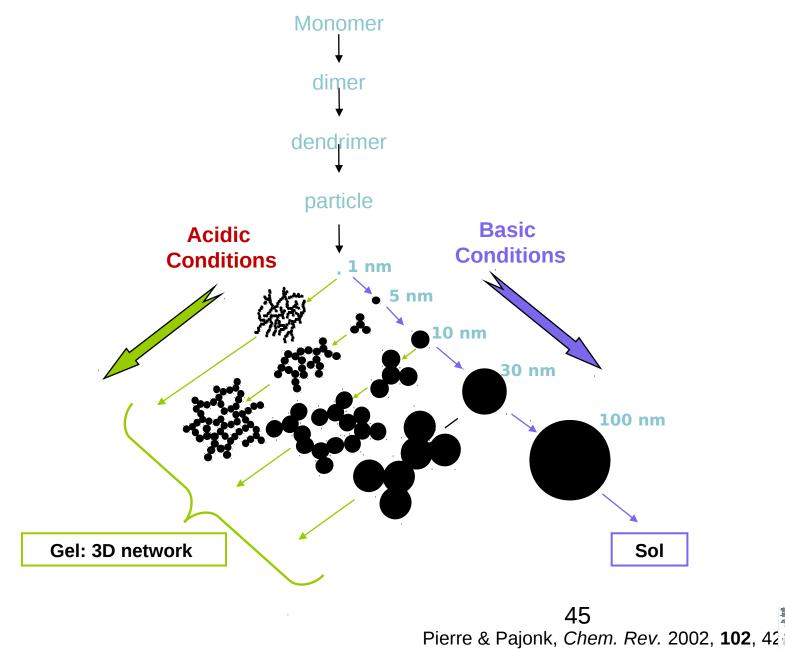
Step 6: Densification and decomposition of the gels at high temperatures (T>8000C).

The pores of the gel network are collapsed, and remaining organic species are volatilized. The typical steps that are involved in sol-gel processing are shown in the schematic diagram below.









CSIC

